



INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

<p>(51) International Patent Classification ⁶ : A61F 2/16</p>	<p>A1</p>	<p>(11) International Publication Number: WO 99/33411</p> <p>(43) International Publication Date: 8 July 1999 (08.07.99)</p>
<p>(21) International Application Number: PCT/GB98/03917</p> <p>(22) International Filing Date: 29 December 1998 (29.12.98)</p> <p>(30) Priority Data: 9727316.3 29 December 1997 (29.12.97) GB 9801214.9 22 January 1998 (22.01.98) GB</p> <p>(71) Applicant (for all designated States except US): DUCK-WORTH & KENT LIMITED [GB/GB]; 7 Marquis Business Centre, Royston Road, Baldock, Hertfordshire SG7 6XL (GB).</p> <p>(72) Inventor; and (75) Inventor/Applicant (for US only): WALDOCK, Terence, Arnold [GB/GB]; The Manor House, Church Road, Meppershall, Bedfordshire SG17 5NA (GB).</p> <p>(74) Agent: THOMSON, Roger, Bruce; W. P. Thompson & Co., Eastcheap House, Central Approach, Letchworth, Hertfordshire SG6 3DS (GB).</p>		<p>(81) Designated States: AU, BR, CA, GB, JP, RU, US, European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE).</p> <p>Published <i>With international search report.</i></p>
<p>(54) Title: INJECTORS FOR INTRAOCULAR LENSES</p> <div data-bbox="318 1178 1263 1444" data-label="Image"> </div> <p>(57) Abstract</p> <p>An instrument for the insertion of an intraocular lens into an eye comprises a body portion (10), a nose portion (14) through which runs a passage for the lens to pass to a dispensing tip, and a plunger (12). The nose portion (14) is pivotally connected to the body portion (10) so that the barrel can be broken open for the placement of the lens into the nose portion. The lens is preferably placed on two spaced parallel nose pins to facilitate its folding. A cross pin preferably straddles the nose pins and under which the lens is arranged to pass, to prevent lifting and tilting of the lens.</p>		

FOR THE PURPOSES OF INFORMATION ONLY

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AL	Albania	ES	Spain	LS	Lesotho	SI	Slovenia
AM	Armenia	FI	Finland	LT	Lithuania	SK	Slovakia
AT	Austria	FR	France	LU	Luxembourg	SN	Senegal
AU	Australia	GA	Gabon	LV	Latvia	SZ	Swaziland
AZ	Azerbaijan	GB	United Kingdom	MC	Monaco	TD	Chad
BA	Bosnia and Herzegovina	GE	Georgia	MD	Republic of Moldova	TG	Togo
BB	Barbados	GH	Ghana	MG	Madagascar	TJ	Tajikistan
BE	Belgium	GN	Guinea	MK	The former Yugoslav Republic of Macedonia	TM	Turkmenistan
BF	Burkina Faso	GR	Greece	ML	Mali	TR	Turkey
BG	Bulgaria	HU	Hungary	MN	Mongolia	TT	Trinidad and Tobago
BJ	Benin	IE	Ireland	MR	Mauritania	UA	Ukraine
BR	Brazil	IL	Israel	MW	Malawi	UG	Uganda
BY	Belarus	IS	Iceland	MX	Mexico	US	United States of America
CA	Canada	IT	Italy	NE	Niger	UZ	Uzbekistan
CF	Central African Republic	JP	Japan	NL	Netherlands	VN	Viet Nam
CG	Congo	KE	Kenya	NO	Norway	YU	Yugoslavia
CH	Switzerland	KG	Kyrgyzstan	NZ	New Zealand	ZW	Zimbabwe
CI	Côte d'Ivoire	KP	Democratic People's Republic of Korea	PL	Poland		
CM	Cameroon	KR	Republic of Korea	PT	Portugal		
CN	China	KZ	Kazakhstan	RO	Romania		
CU	Cuba	LC	Saint Lucia	RU	Russian Federation		
CZ	Czech Republic	LI	Liechtenstein	SD	Sudan		
DE	Germany	LK	Sri Lanka	SE	Sweden		
DK	Denmark	LR	Liberia	SG	Singapore		
EE	Estonia						

INJECTORS FOR INTRAOCULAR LENSES

This invention relates to instruments for inserting an intraocular lens into an eye. It is necessary in certain ophthalmic surgical procedures to insert an intraocular lens through a small incision, such as in the phacoemulsification technique of removing cataracts.

One particular instrument for carrying out this procedure is described in US patent 4,681,102 (Bartell). In this instrument the intraocular lens is placed within a hinged, generally cylindrical load chamber having a pair of flanges. The load chamber is folded around the intraocular lens, so that the lens itself becomes folded or rolled along its length. The load chamber is fitted into an injector portion which has a slot which is keyed to the flanges of the load chamber. The injector portion and load chamber are then fitted into an insertion cone which defines a lumen for passage of the lens through the lumen. A plunger which is inserted into the injector portion is then used to push the lens through the lumen and into the eye. The folded intraocular lens opens out into its flattened form as it emerges from the distal end of the insertion cone.

In US 4,681,102 the insertion cone, the load chamber and the injector portion are all separate pieces, preferably made of moulded plastics material, so that they can be disposed of after a single use. This means of course that there is a continuing expense in the use of the instrument and it is also necessary to have available a supply of parts.

It is an object of the present invention to provide an instrument for the insertion of intraocular lenses which does not involve the use of disposable parts.

It is a further object of the present invention to provide an instrument for the insertion of intraocular lenses in which the lens is not folded within a load chamber.

It is yet a further object of the present invention to
5 provide an instrument for the insertion of intraocular lenses in which the lens can be placed easily into the instrument for subsequent injection.

The instrument of the present invention, dispensing as it does with disposable parts, is adapted for repeated use,
10 with appropriate sterilisation, and can be made for example of titanium or a titanium alloy. One can produce an extremely accurately machined instrument which is easy both to load and to use.

In accordance with the present invention there is
15 provided an instrument for the insertion of an intraocular lens into an eye, which comprises a body portion, a nose portion forward of the body portion and having a lumen through which the lens is arranged to pass, and a plunger movable through the body portion and the nose portion, wherein the
20 nose portion is pivotally connected to the body portion for the receipt of an intraocular lens therein in a pivotally opened position.

Preferably, the nose portion is hingedly connected to the forward end of the body portion and is movable between open
25 and closed positions in a manner similar to the opening and closing of a shotgun barrel. In the broken open position the lens can be inserted and then the nose portion is closed and locked into place for the operation then of the plunger to dispense the lens from the nose portion.

30 In a preferred embodiment, the lumen or internal channel through the nose portion reduces in cross-section in a

smoothly continuous way so that as the lens passes deeper into the nose portion it is constrained to fold for dispensation through the tip of the nose portion.

According to a further preferred feature of the invention, the nose portion is pivotally mounted on a forward extension of the body portion, so that the hinge position is forward of the body portion and so that the nose portion, when in the open position, is spaced from the body portion to facilitate the placement of a lens into position in the nose.

10 It is a further object of the present invention to provide an instrument for the insertion of intraocular lenses in which the lens which is to be inserted is laid on support means which not only serves as a guide for the lens in its onward movement through the nose, but also facilitates the positioning of the lens correctly within the instrument.

In accordance with a preferred embodiment of the present invention there is provided an instrument for the insertion of an intraocular lens into an eye wherein there is provided support means for the lens which defines an undulating support surface for the lens.

Preferably, the support means comprises two parallel spaced nose pins whose surfaces define the undulating support surface for the lens.

The pins are preferably set into the rear end of the nose portion of the instrument.

The advantage of an undulating support surface for the lens, for example as provided by the two pins, is that this configuration also helps to centralise the forceps which are used to place the lens within the instrument. Additionally, 30 the use of two spaced pins or an equivalent surface configuration helps to guide the lens into the funnel or lumen

through which the lens has to pass. The space between the two pins, or the valley in some other equivalent configuration, allows the lens more easily to fold about its centre as it is pushed forward through the nose portion of the instrument.

5 Preferably the instrument includes a cross pin extending transversely across the path of the lens and beneath which the lens is arranged to pass. Preferably, the cross pin straddles the nose pins. The main purpose of the cross pin is to prevent lifting or tilting of the lens both on insertion into
10 the nose and in its passage towards the tip.

In order that the invention may be more fully understood, a number of preferred embodiments of lens injector in accordance with the invention will now be described by way of example and with reference to the accompanying drawings. In
15 the drawings:

Fig. 1a shows a plan view of a first embodiment of injector in accordance with the invention, in the closed position;

Fig. 1b is the side view of the injector of Fig. 1a;

20 Fig. 2 shows the injector according to Fig. 1b, but with the injector in the opened position;

Fig. 3 shows internal details of the lens injector of Figs. 1 and 2, and is shown with the plunger fully depressed;

Fig. 4 shows the lens injector of Fig. 3, in side view,
25 and with the plunger retracted;

Fig. 5 shows the lens injector of Fig. 4, but from below;

Fig. 6 is a plan view of the main body of the lens injector;

Fig. 7 is the side view of the main body of the lens
30 injector shown in Fig. 6;

Fig. 8 is a side view of the plunger and push rod of the

lens injector;

Fig. 9 is the view of the plunger and push rod of Fig. 8, from below;

Fig. 10 is the view on arrow A in Fig. 9;

5 Fig. 11 is the front end view of the push rod, viewed from the left-hand end as shown in Fig. 10;

Fig. 12 is a plan view of the two-part nose assembly of the lens injector;

Fig. 13 is the side view of the nose assembly shown in 10 Fig. 12;

Fig. 14 is the underneath plan view of the nose assembly shown in Figs. 12 and 13;

Fig. 15 shows the front portion of the nose assembly, in top plan view;

15 Fig. 16 shows the front portion of the nose assembly of Fig. 15, in side view;

Fig. 16a is the view on the right-hand end of Fig. 16;

Fig. 17 shows the front portion of the nose assembly of Figs. 15 and 16, in underneath plan view;

20 Figs. 18, 19 and 20 are plan, side and underneath plan views respectively of the outer sleeve which in combination with the front portion shown in Figs. 15 to 17 forms the nose assembly shown in Figs. 12 to 14;

Fig. 21 is a side view of a second embodiment of lens 25 injector in accordance with the invention, with the plunger retracted;

Fig. 22 shows the lens injector of Fig. 21, but from below;

Fig. 23 is the top plan view of the lens injector of Fig. 30 21, with the plunger fully depressed;

Fig. 24 is the side view of the front piece of the nose

portion of the lens injector;

Fig. 25 is the end view taken in the direction of the arrow XXV in Fig. 24;

Fig. 26 is the plan view of the front piece of the nose
5 portion shown in Fig. 24;

Fig. 27 is the side view of the complete nose assembly of the nose injector, including an outer sleeve;

Fig. 28 is the end view taken in the direction of the arrow XXVIII in Fig. 27;

10 Fig. 29 is the top plan view of the nose assembly of Fig. 27;

Fig. 30 is the underneath plan view of the nose assembly shown in Fig. 27;

Fig. 31 shows one of the pins used in the nose assembly;

15 Fig. 32 is the top plan view of a modified embodiment of nose assembly, illustrating the use of a cross pin in the lens passage;

Fig. 33 is the side view of the nose assembly of Fig. 32;

Fig. 34 is the end view of the nose assembly of Figs. 32
20 and 33 taken from the right-hand end of Fig. 33;

Fig. 35 is the side view of an alternative embodiment of nose for a lens injector according to the invention;

Fig. 36 is the top plan view of the nose of Fig. 35;

Fig. 37 is the end view of the nose of Fig. 35 taken from
25 the right-hand end of Fig. 35;

Fig. 38 shows the pin support which is fitted into the rear end of the nose of Figs. 35 to 37;

Fig. 39 shows the pin support of Fig. 38 fitted with two nose pins to make a nose pin assembly;

30 Fig. 40 is a side view of the nose pin assembly of Fig. 39; and,

Fig. 41 is the sectional view on XLI-XLI in Fig. 39.

A first embodiment of intraocular lens injector of the present invention is shown generally in Figs. 1a, 1b and 2. It will be seen that the injector essentially comprises a body 5 portion 10, a plunger 12 and a nose portion 14. Each of these parts will be described in more detail hereinafter. As will be apparent from these Figures, the nose portion 14 can be "broken open" in like manner to a shotgun barrel. In the closed position as shown in Figs. 1a and 1b the nose portion 10 14 is coaxial with the main body 10 and the plunger 12. Fig. 2 shows the nose portion broken open. The body portion 10 has a finger 16 projecting from the front end of the body at the bottom of the body, and a pivot pin 18 extends through the nose portion and the finger 16 to provide the pivotal 15 mounting. As shown in Fig. 2, the nose portion is pivotable through 90° from the open position to the closed position and vice versa. It will be seen in Fig. 1a that the nose portion and body portion are each provided with an engraved marking 20, with the markings being in alignment when the nose portion 20 is closed. These lines provide an indication to the user as to where the nose portion should be pushed in order to open the nose.

Although the method of operation of the instrument will be described in more detail hereinafter, it will be helpful 25 briefly to describe the method of use with reference to Figs. 1a, 1b and 2. From the closed position shown in Figs. 1a and 1b the injector is opened by holding the instrument with the engraved lines 20 uppermost and pushing down on the nose 14. With the nose portion thus opened, the intraocular lens to be 30 inserted into the eye is placed into the nose in the direction of the arrow A in Fig. 2, using suitable forceps. The lens

is slid forward on the flat face at the bottom of the nose, as will become evident from the later drawings of this embodiment. In the case of a haptic lens, when the rear haptic is fully into the nose, the nose is closed until it 5 clicks shut. The plunger is then depressed, causing the lens to be ejected from the tip of the nose portion and through the incision in the eye.

Reference is now made to Figs. 3 to 5, which show more details of the lens injector. The nose portion 14 will be 10 described in more detail hereinafter. Suffice it to say here that there is a passage completely through the nose portion which changes in cross-section and configuration from one end of the nose portion to the other. At the distal end the nose portion has a tip 22 through which the lens is ejected. As 15 shown in Fig. 3, when the plunger 12 is fully depressed, the push rod 24 passes out through the tip of the nose portion. The plunger 12 is slidable within the body portion 10 which is in the form of a cylindrical barrel having a bore therethrough. At two positions along its length the plunger 20 12 has circumferential grooves 26 (Fig. 8) which carry bushes 28 which have the purpose of steadying the plunger 12 as it is moved slidably within the barrel. A spring 30 provides a force against which the plunger is depressed and urges the plunger 12 into its retracted position. The spring 30 is 25 seated at one end against an annular face inside the front end of the barrel and at the other end against a forwardly facing annular surface 32 (Fig. 8) at the forward end of the plunger 12. The underside of the plunger 12 is provided with a longitudinally extending groove 34. A stop pin 36 which 30 extends radially through the wall of the body portion 10 at its rearward end projects into the groove 34 in the plunger

12 and serves as a stop to limit movement of the plunger both forwards and rearwards.

The push rod which is indicated generally at 24 is fitted into the forward end of the plunger 12. A hole is drilled in the plunger and the push rod is held in position by friction welding. The push rod 24 is of such a length that when the plunger 12 is fully retracted, as shown in Figs. 4 and 5, the leading end of the push rod lies within the forward end of the body portion 10 and rearwardly of the nose portion 14. This enables the nose portion 14 to be broken open without danger of striking against the end of the push rod. As shown most clearly in Fig. 4, the leading end of the push rod 24 is located at the bottom of a counterbore 38 through the forward end of the body portion 10. Referring now to Figs. 6 and 7, these show the body portion 10 in more detail. In particular, they show the forwardly projecting finger 16 at the leading end of the barrel and which is provided with a hole 40 therethrough to receive the pivot pin 18. At the rear end of the barrel, in Fig. 7, is shown a hole 42 into which the stop pin 36 is fitted.

Figs. 8 to 11 show more details of the plunger 12 and push rod 24. The leading end of the push rod 24 is specially shaped, as shown most clearly in Figs. 10 and 11, in order to enable the lens to be folded and pushed reliably and effectively through the nose portion and into the eye. The lens injector of the present invention can be used both with plate-type lenses and with haptic lenses. The shape of the push rod at its leading end is designed so that it will slide through the lumen in the nose portion 14 by virtue of its curved undersurface and yet will safely guide the lens through the lumen.

Figs. 12 to 14 show details of the nose assembly which is indicated generally at 14. The nose assembly is made in two parts, a front piece which is shown in Figs. 15 to 17 and an outer sleeve which is shown in Figs. 18 to 20. The front 5 portion shown in Figs. 15 to 17 includes the tip 22 which is cut off at 45° at the distal end. Behind the generally cylindrical but slightly tapering tip 22 is a frusto-conical portion 44. To the rear of that is a shaped portion 46 which includes a "bullet-shaped" recess 48 and a tapered bore 10 indicated at 50 in Fig. 16. Shaping the rear portion 46 in this way causes the lens which is inserted here to be folded as it is pushed forward by the push rod into the cylindrical passage 52 through the tip 22. The folding of the lens is effected solely by the shape of the encircling passageway and 15 only begins when the lens begins its movement through the nose portion.

The outer sleeve shown in Figs. 18 to 20 comprises a generally cylindrical sleeve 54 which fits over the rear portion 46 of the front piece of the nose and which abuts the 20 annular rearwardly facing surface 56 of the frusto-conical portion 44. The outer sleeve 54 is provided with a hole 56 therethrough which receives the pivot pin 18. The rearward end of the sleeve 54 is provided with a rearwardly projecting spigot 58 which is recessed as indicated at 60 to serve as a 25 latch for a locking pin when the nose portion is closed against the body portion.

The whole instrument which comprises the lens injector is preferably made of titanium or a titanium alloy. This material can be machined to great accuracy and with a good 30 surface finish. It can also be easily sterilised for repeated use.

The injector shown in Figs. 21 to 31 essentially comprises a body portion 110, a plunger 112 and a nose portion 114. The nose portion 114 can be "broken open" in like manner to a shotgun barrel, as described in the preceding embodiment. 5 In the closed position, as shown in Figs. 21 to 23, the nose portion 114 is coaxial with the main body 110 and the plunger 112. As will be described in more detail hereinafter, with the plunger 112 retracted as shown in Figs. 21 and 22, the nose portion 114 is broken open and the lens which is to be 10 inserted into the eye is placed in the nose, using suitable forceps. In the present embodiment, the lens is inserted into the open rear end of the nose portion of the injector, using suitable forceps. The nose is then closed until it clicks shut. Subsequently the plunger is depressed, causing the lens 15 to be ejected from the tip of the nose portion and through an incision in the eye.

In the present embodiment, the nose portion 114 is provided with a "window" 116 which is open to the chamber into which the lens is placed. This is simply a viewing window 20 which enables the surgeon to see the lens in place. It also enables the surgeon to check that the rear haptic of an intraocular lens which has haptics is not caught by the front end of the plunger 112.

Reference is now made to Figs. 24 to 26, which show more 25 details of the front piece of the nose assembly. The nose assembly is made in two parts, a front piece which is shown in Figs. 24 to 26, and an outer sleeve which is shown in combination with the front portion in Figs. 27 to 30. The front piece shown in Figs. 24 to 26 includes a tip 118 which 30 is cut off at 45° at the distal end. The tip has a cylindrical internal bore 120 of for example 2.2 mm diameter,

with the external surface being generally cylindrical but slightly tapering. To the rear of the tip 18 is a frusto-conical portion 122. To the rear of that is a stub portion 124 which has a cylindrical external surface. The stub 5 portion 124 has an internal tapered bore 126 which decreases in diameter from the rearward end towards the internal bore 120 in the tip 118. The bore 126 and the bore 120 together form a passage which is of decreasing cross-section from rearward end to forward end, but which is of circular cross- 10 section throughout.

As shown in Figs. 24 to 26, a pair of cylindrical holes 128 are bored into the stub portion 124 and frusto-conical portion 122 of the nose. These bores 128 extend parallel to the longitudinal axis of the nose portion. The forward end 15 of each bore 128 lies approximately halfway along the length of the frusto-conical portion 122 and is contiguous at its periphery with the bore through the nose portion. The rearward end of each hole 128 exits in the sloping surface of the tapered bore 126.

20 As will be seen most clearly from Fig. 24, there is a transition zone in the internal bore, between the rearward tapering bore 126 and the forward cylindrical bore 120, within the frusto-conical portion 122. This transition bore 130 is tapered, but with a lesser taper than that of the rearward 25 bore 126. The front end of each of the holes 128 "merges" with this transitional bore 130.

As will be seen from Figs. 25 and 26, the two holes 128 are spaced apart, each at the same distance from the central vertical plane through the nose portion. They are thus 30 symmetrically positioned in relation to the throughbore 126, 130, 120. Each of the holes 128 shown in Figs. 24 to 26 is

fitted with a cylindrical pin 132 which is shown in Fig. 31. Each pin 132 is cylindrical but has a chamfered rear end 136. A pin 132 is press-fitted into each of the holes 128 in the front piece of the nose portion. The rear end of each pin 5 132, when fitted, lies flush with the rearward end of the stub portion 124 of the front piece of the nose assembly. This is shown most clearly in Figs. 27 to 30, which show the complete nose assembly consisting of the front piece, the two pins 132 and an outer sleeve 134 which is a press fit over the 10 stub portion 124 of the front piece. The forward end of the sleeve 134 abuts the rearward end face of the frusto-conical portion 122. The outer sleeve 134 is provided with the window 116. This is dimensioned so that in use, as shown most clearly in Fig. 29, the two pins 132 can be seen in their 15 side-by-side position below the window. The pivotal connection of the nose portion to the body portion of the instrument has been described earlier and is not repeated here.

In use, the intraocular lens which is to be inserted into 20 the eye, whether with or without haptics, is inserted into the nose portion of the injector by first pivoting open the nose assembly and then inserting the lens, using forceps, from the rear end of the nose assembly through the open aperture which is there. Using the forceps, the lens is laid upon the two 25 pins 132 in a sufficiently forward position that the rear haptic of the lens is forward of the rearward end of the nose assembly, so that it does not become caught when the nose assembly is closed to the main body. The provision of the two spaced pins 132 lends itself to the use of forceps to 30 insert the lens. By using a pair of forceps which are essentially T-shaped in cross-section, the stem of the T can

be slid between the two pins which will automatically centre the forceps within the chamber and guide the forceps and the lens forward until the lens is released and the forceps are withdrawn. This facilitates the insertion of the lens into
5 the chamber.

In use, the intraocular lens is placed on the upper surface of the two pins. It is therefore supported on the two arcuate surfaces. When the lens is to be injected, the plunger 112 is depressed and the forward end of the plunger
10 enters the chamber in the nose assembly at the level which enables it to slide forward over the pins 132, pushing the lens forward as it travels. As the lens passes forward through the bores 126, 130, 120, so it will be folded by the shape of the encircling circular cross-section passageway.
15 The two pins 132 guide the lens while it passes through the tapering bores 126 and 130, and only terminate their guiding function when the lens enters the cylindrical bore 120 in the tip 118. A further feature of this arrangement is that because of the spacing of the two pins 132, with what is
20 effectively a valley between them, as the lens is folded by the encircling walls, this folding is enhanced by a tendency for the central zone of the lens to sink into the valley between the pins and thus to ensure that the folding is symmetrical about the centre.

25 The whole instrument which comprises the lens injector is preferably made of titanium or a titanium alloy. This material can be machined to great accuracy and with a good surface finish. It can also be easily sterilised for repeated use. There are no disposable parts involved. The
30 use of pins 132 is not a problem with a metal instrument, such as one made of titanium. It simply requires two holes to be

bored in the nose piece and for the pins then to be fitted before the rest of the nose is assembled. This does not involve any complicated machining operations. However, particularly if alternative materials are used for the instrument, one could replace the pins by an internal configuration for the chamber within the nose assembly which is undulating and shaped to give the guiding and folding functions described above. For example, the lower portion of the internal chamber could be of undulating shape defining two arcuate peaks upon which the lens would be seated, in a manner analogous to that of the two pins 132.

Various alternative means of achieving the same functions as described above will be apparent to those skilled in this art. For example, instead of fitting pins into drilled holes in the nose assembly one could provide a suitably shaped insert arranged to be fitted into the chamber, with this insert again having a suitable seating surface configuration to provide the positioning and guiding functions described above. However, it has been found that the use of pins is a simple yet effective way of achieving the objects of the invention, particularly with a lens injector which is designed for repeated use.

Referring now to Figs. 32 to 34, these show a modification of the nose, which can be used with any of the embodiments of the invention. The nose assembly 200 is here shown without the two nose pins, shown in Figs. 27 to 30, although bores 202 for the nose pins are shown. The pivot pin for the pivoting of the nose assembly is here shown at 204. In this embodiment a pair of bores 206a, 206b are provided through the nose substantially midway along the length of the window 208 to receive a cross pin 210 which when fitted

extends transversely across the direction of travel of the lens and at right-angles to the nose pins. The cross pin 210 is positioned straddling the nose pins so that when the lens is set in place using forceps the lens rests on the nose pins 5 with its front edge under the cross pin. When the lens is pushed in under the cross pin, using the forceps, this starts the lens folding process. The cross pin 210 also prevents any possibility of the lens rising or tilting when it is inserted. Specially designed forceps can be used so that when the 10 forceps strike the cross pin the user knows that the lens is correctly positioned and can be released.

After the lens has been set in place, the nose portion is pivoted into its closed position and the plunger can be operated to engage the lens and push it forwards, folding as 15 it advances. The plunger is arranged just to pass beneath the cross pin 210 in its forward movement.

A further advantage of the use of two nose pins is that when using a lens having two haptics, the rear haptic drops down below the adjacent nose pin and therefore is never in the 20 line of movement of the plunger and cannot become caught up by the plunger. This means that the double nose pin arrangement works much better than using a flat receiving plate or other surface for this lens.

Figs. 35 to 41 show yet a further modification to the 25 nose of the lens injector. The nose indicated generally at 300 is of generally the same configuration as those described earlier. It includes a pivot pin 302 to enable the barrel to be broken open. In this embodiment however there is no viewing window as in some earlier embodiments. There is 30 however a cross pin 304 which is rivetted into a pair of bores 306a, 306b. In this embodiment, instead of fitting the two

nose pins into holes drilled in the material of the nose, the nose pins 308 are carried by a pin support 310 which is itself fitted into the rear of the nose. The pin support 310 has two arcuate recesses 312 into which the nose pins 308 are seated.

5 The pin support 310 also has two bores 314 adjacent to its respective ends, to enable it to be retained in the nose. As shown most clearly in Figs. 39 and 40, the nose pins 308 rest proud of the surface of the pin support 310 to enable the lens to be deposited thereon. The underside 312 of each nose pin

10 308 is shaped, for example by a turning operation, so as to match exactly the contours of the bore through the nose. There is thus intimate contact between the pin surface 312 and the bore.

CLAIMS

1. An instrument for the insertion of an intraocular lens into an eye, which comprises a body portion, a nose portion forward of the body portion and having a lumen through
5 which the lens is arranged to pass, and a plunger movable through the body portion and the nose portion, wherein the nose portion is pivotally connected to the body portion for the receipt of an intraocular lens therein in a pivotally opened position.
- 10 2. An instrument according to claim 1, in which the nose portion is hingedly connected to the forward end of the body portion and is movable between open and closed positions in the manner of the opening and closing of a shotgun barrel.
3. An instrument according to claim 2, in which the
15 nose portion can be locked into place in the closed position.
4. An instrument according to claim 2 or 3, in which the nose portion is pivotally mounted on a forward extension of the body portion, so that the hinge position is forward of the body portion and so that the nose portion, when in the
20 open position, is spaced from the body portion to facilitate the placement of a lens into position in the nose portion.
5. An instrument according to any preceding claim, in which the lumen through the nose portion reduces in cross-section in a smoothly continuous manner so that as the lens
25 passes deeper into the nose portion it is constrained to fold for dispensation through the tip of the nose portion.
6. An instrument according to any preceding claim, in which there is provided in the nose portion support means for the lens which defines an undulating support surface for the
30 lens.
7. An instrument according to claim 6, in which the

support means comprises two parallel spaced nose pins whose surfaces define the undulating support surface for the lens.

8. An instrument according to claim 7, in which the nose pins are set directly into bores made in the material of
5 the nose portion.

9. An instrument according to claim 7, in which the nose pins are carried by a support member fixed into the rear of the nose portion, with the upper surfaces of the pins being proud of the surface of the support member, and with the
10 undersides of the pins matching the contours of the lumen and being in contact therewith.

10. An instrument according to any preceding claim, which includes a cross pin extending transversely across the path of the lens and beneath which the lens is arranged to
15 pass.

11. An instrument according to claim 10 when dependent on claim 7, 8 or 9, in which the cross pin straddles the nose pins.

12. An instrument according to any preceding claim, in
20 which the nose portion includes a viewing window for the lens.

13. An instrument according to any preceding claim, which is made from titanium or a titanium alloy.

1/13

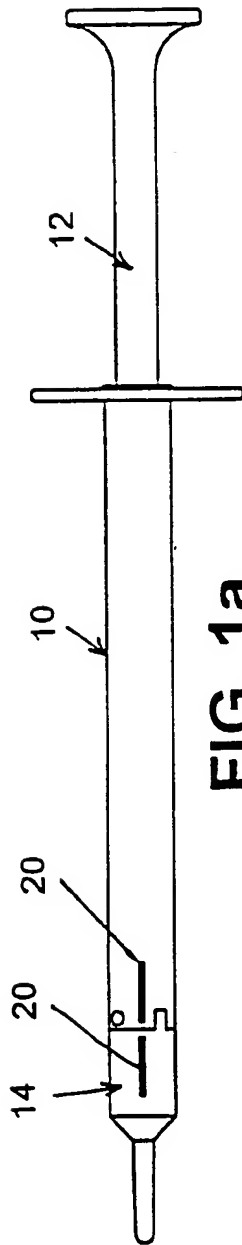


FIG. 1a

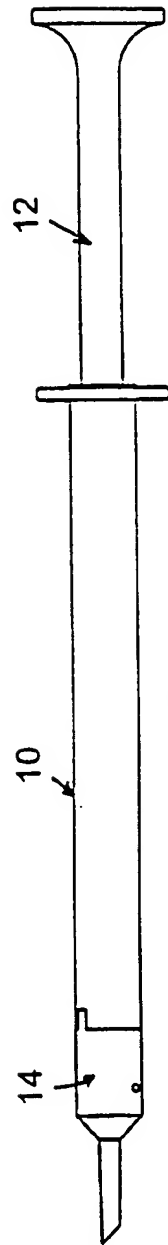


FIG. 1b

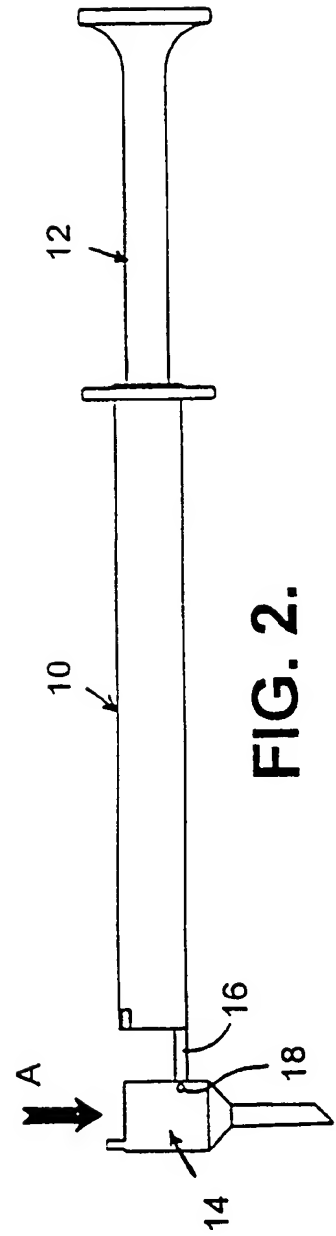


FIG. 2.

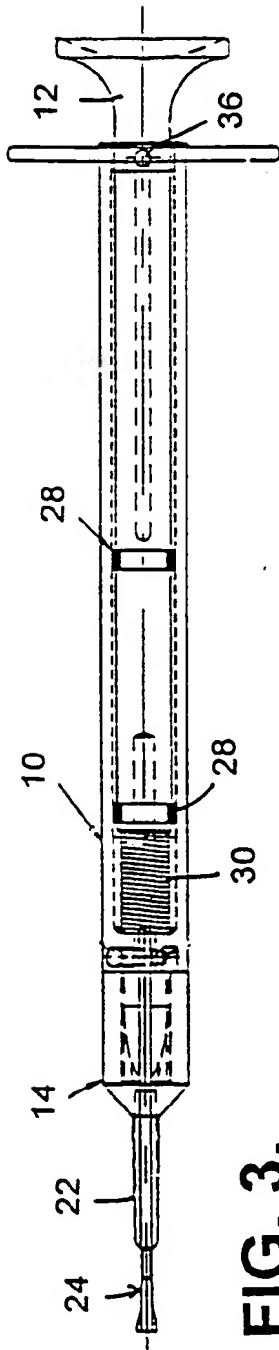


FIG. 3.

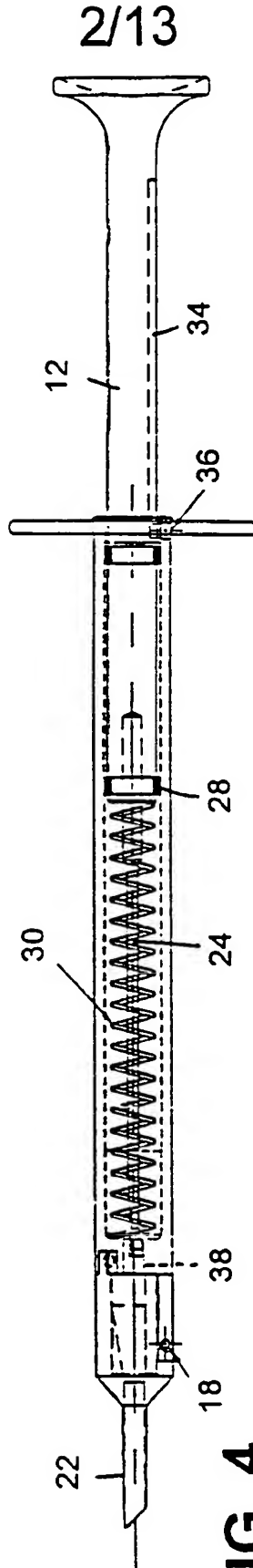


FIG. 4.

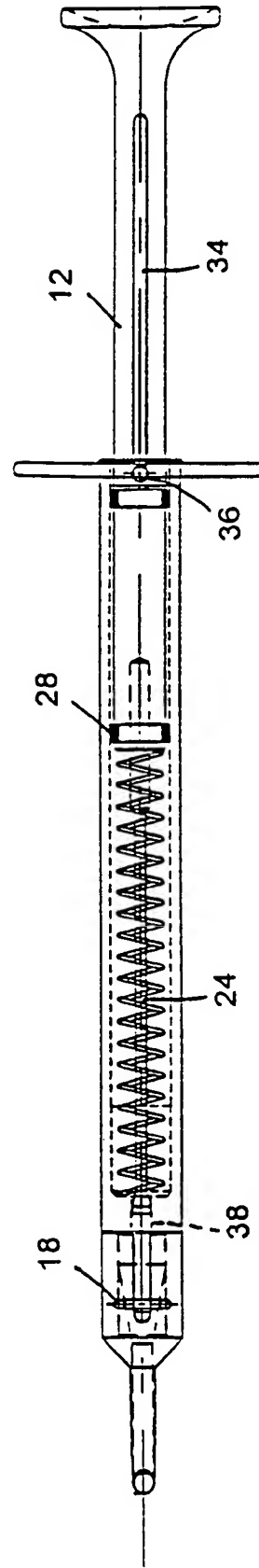


FIG. 5.

3/13

FIG. 6.

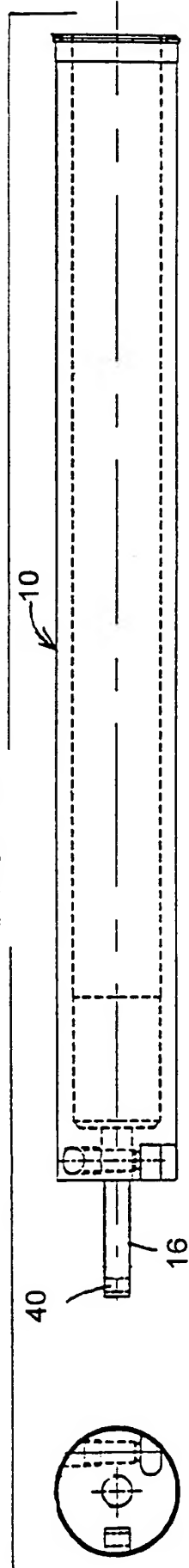


FIG. 7.

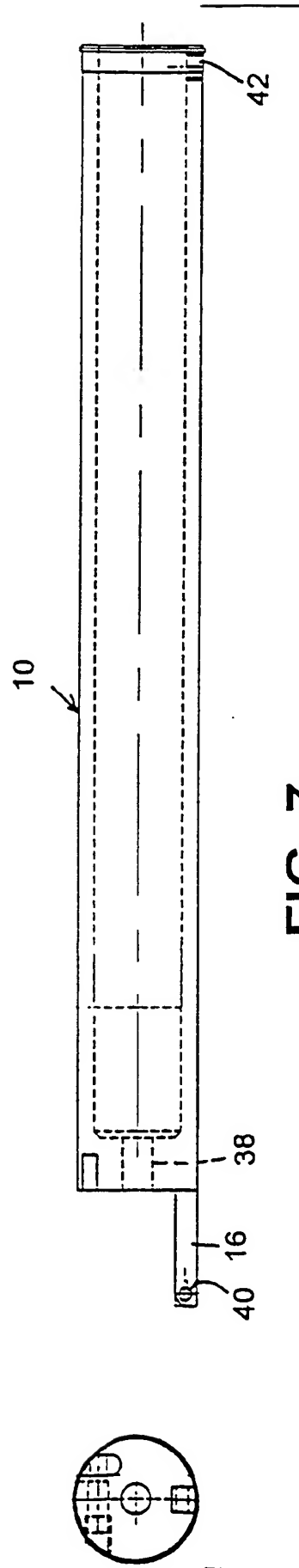


FIG. 8.

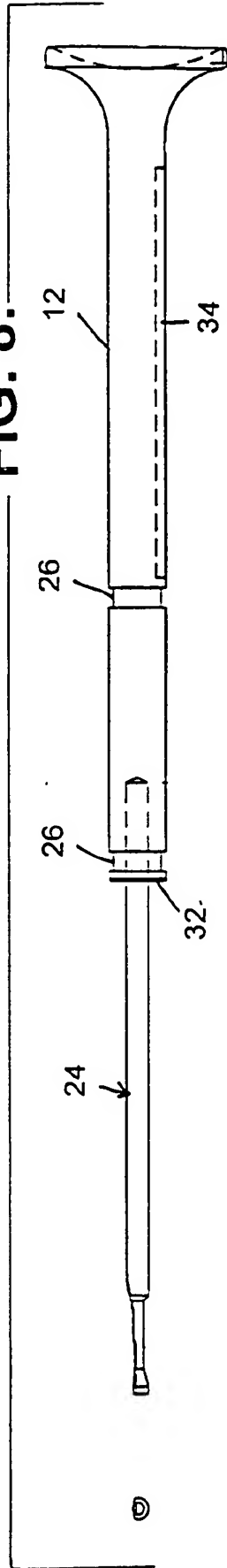
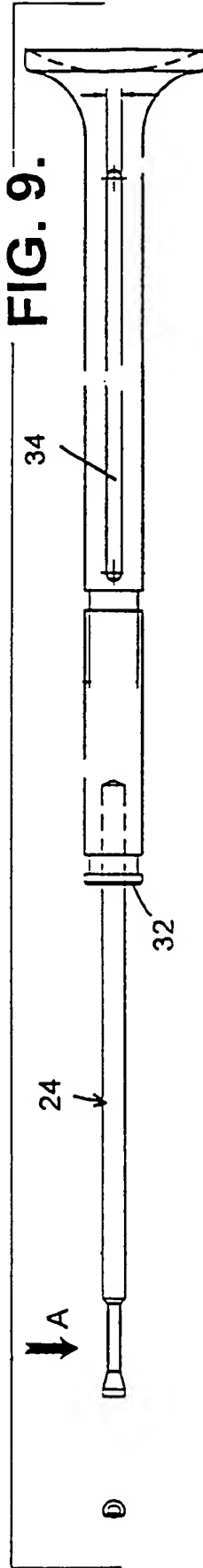


FIG. 9.



4/13

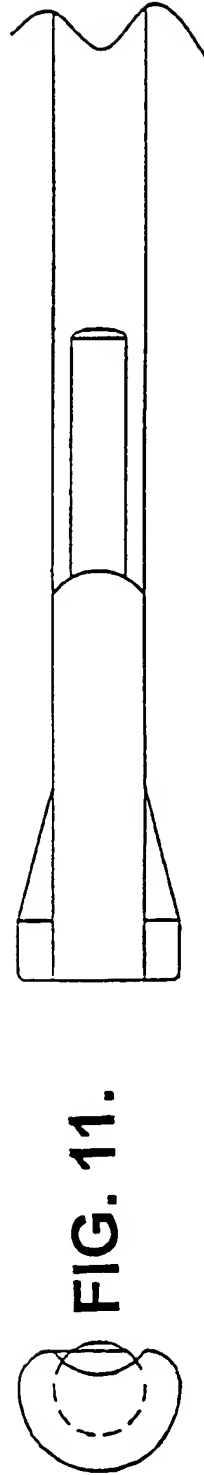
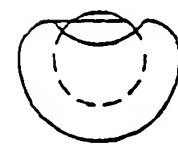


FIG. 10.

FIG. 11.



5/13

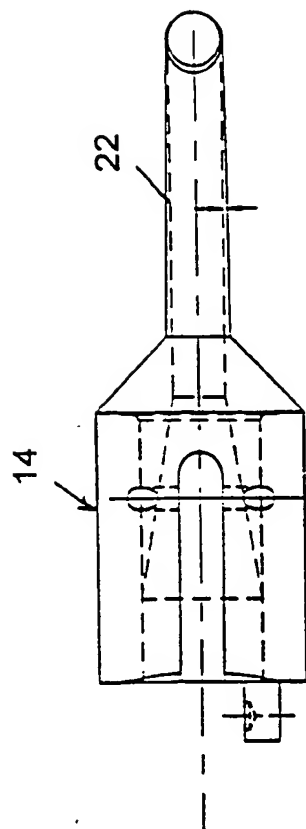


FIG. 14.

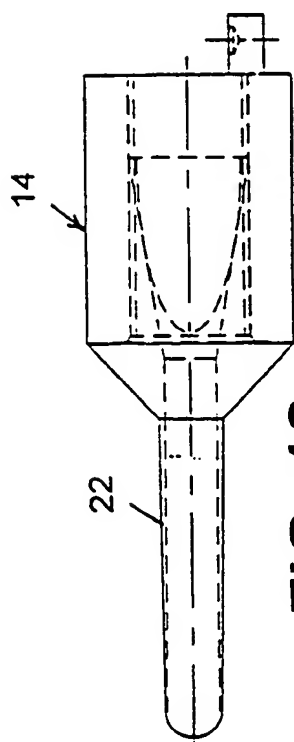


FIG. 12.

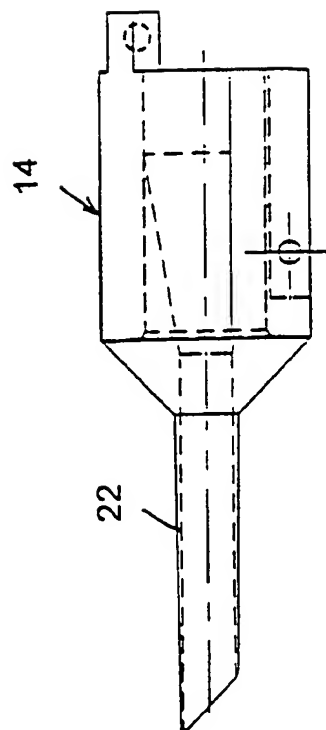


FIG. 13.

FIG. 17.

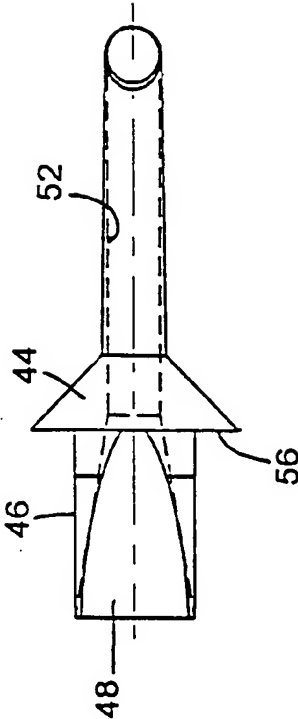


FIG. 15.

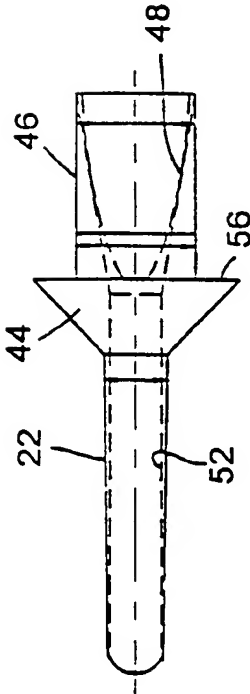


FIG. 16a.

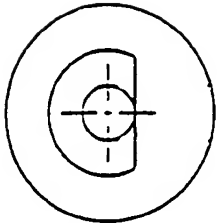
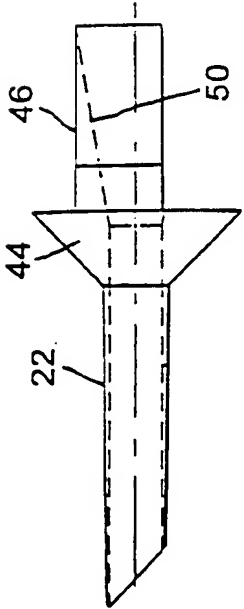


FIG. 16.



7/13

FIG. 18.

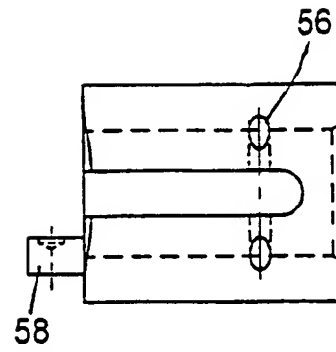
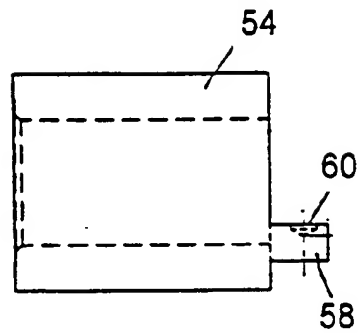


FIG. 20.

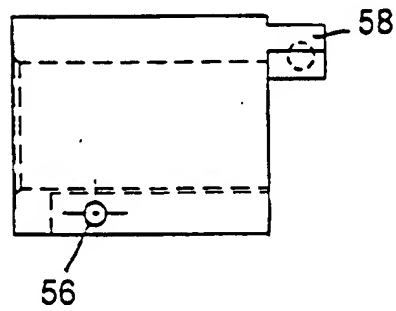
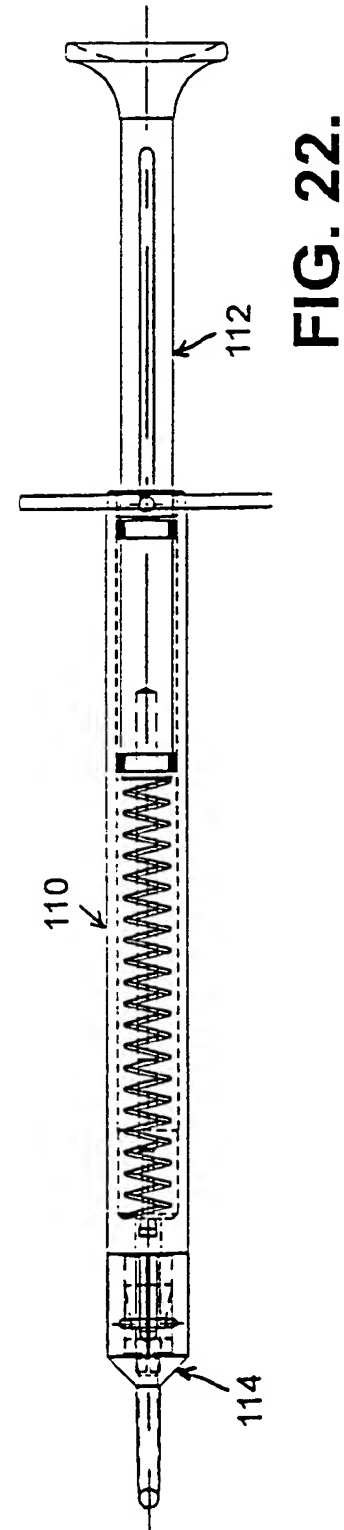
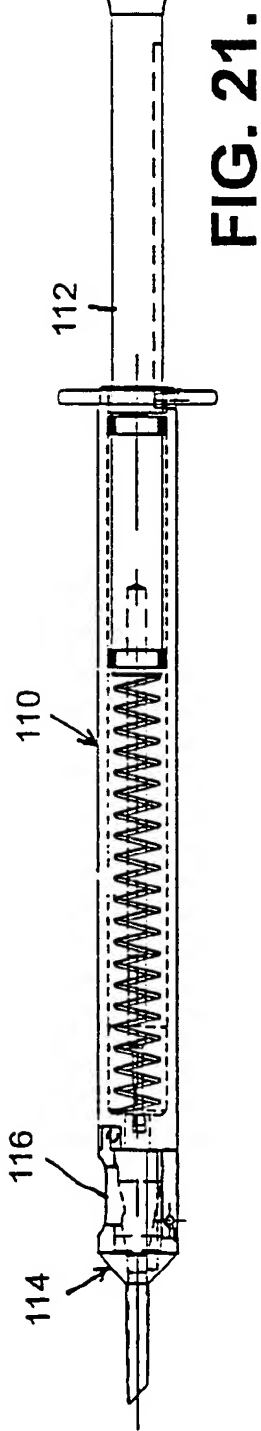
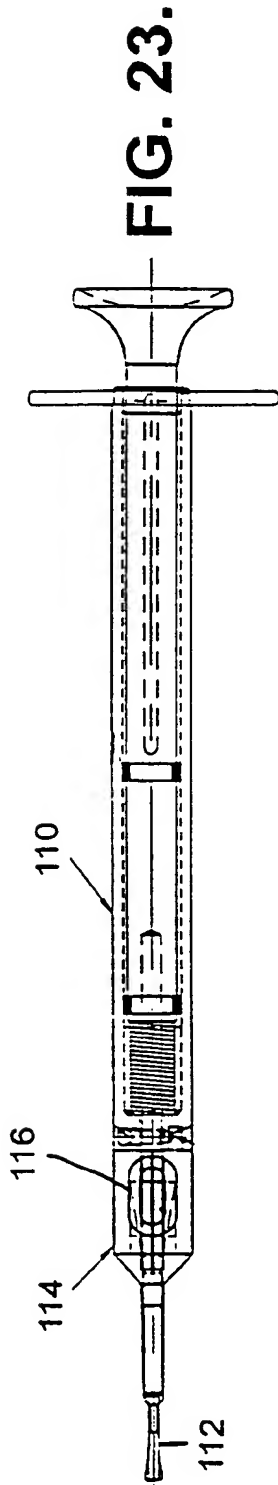


FIG. 19.

8/13



9/13

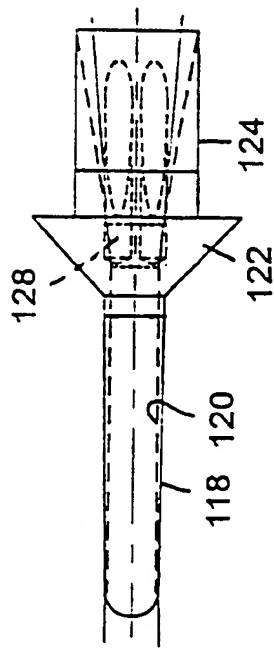


FIG. 26.

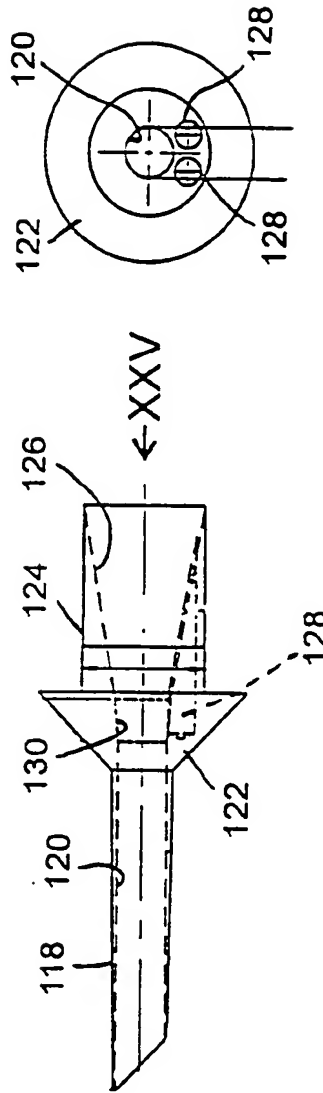


FIG. 24.

FIG. 25.

10/13

FIG. 29.

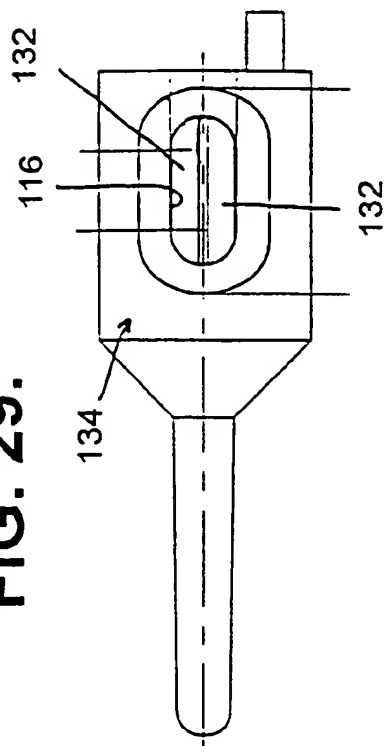


FIG. 30.

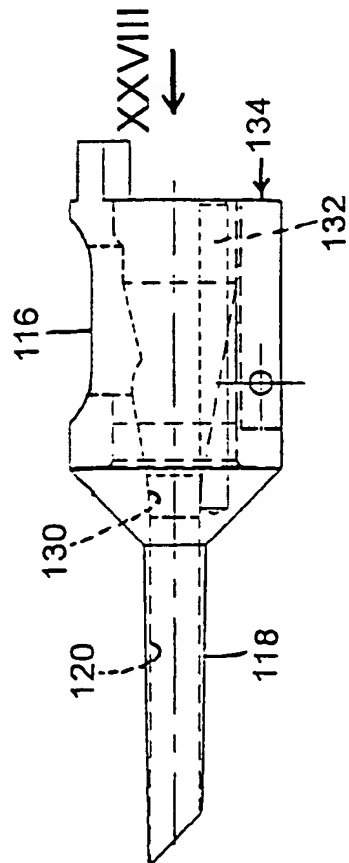
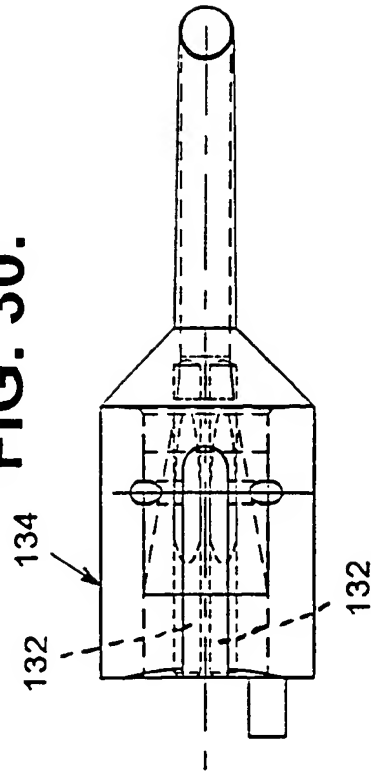


FIG. 27.

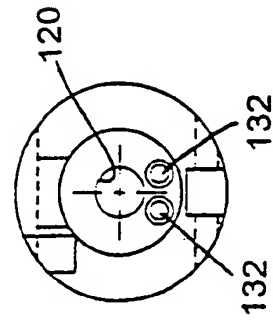


FIG. 28.

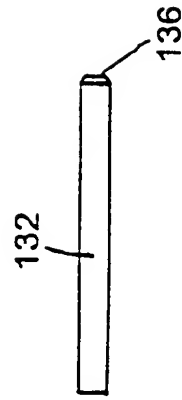


FIG. 31.

FIG. 32.

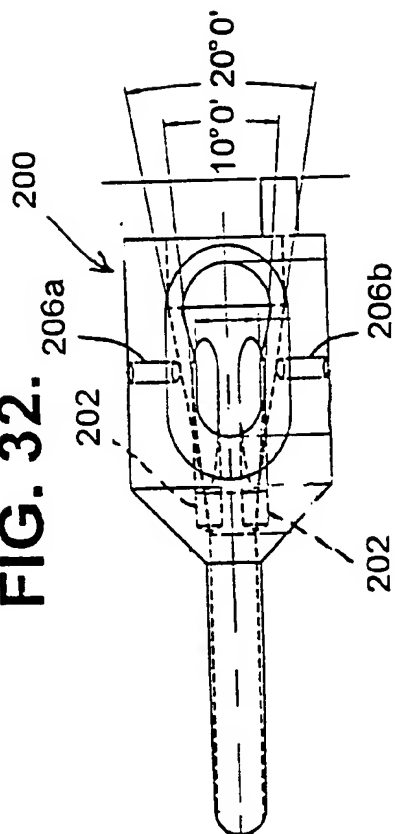


FIG. 34.

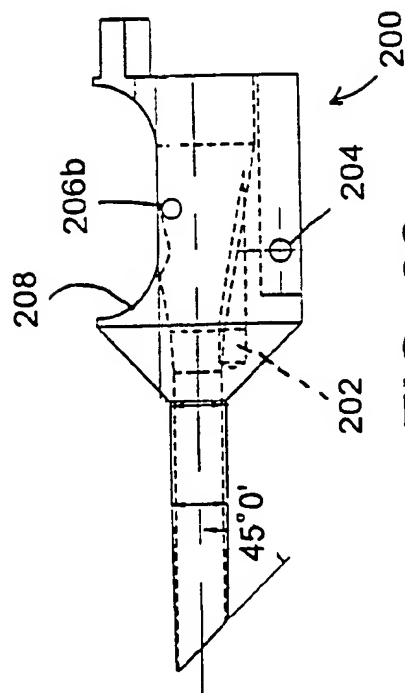
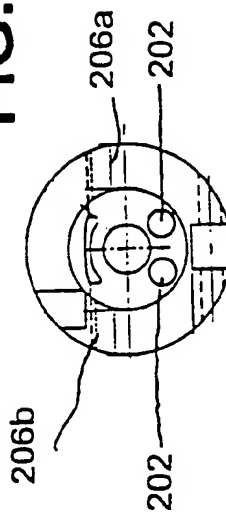


FIG. 33.

12/13

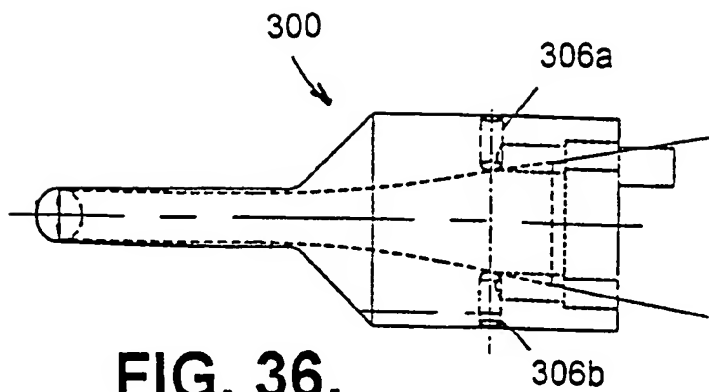


FIG. 36.

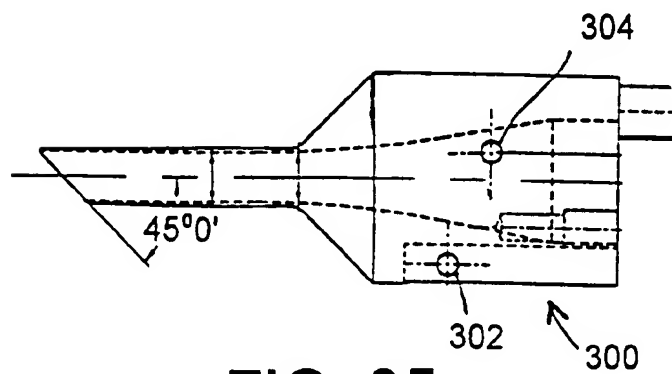


FIG. 35.

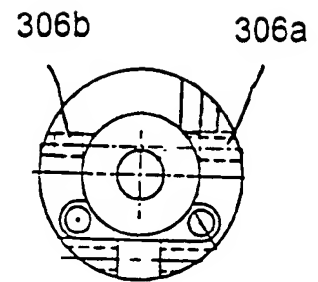


FIG. 37.

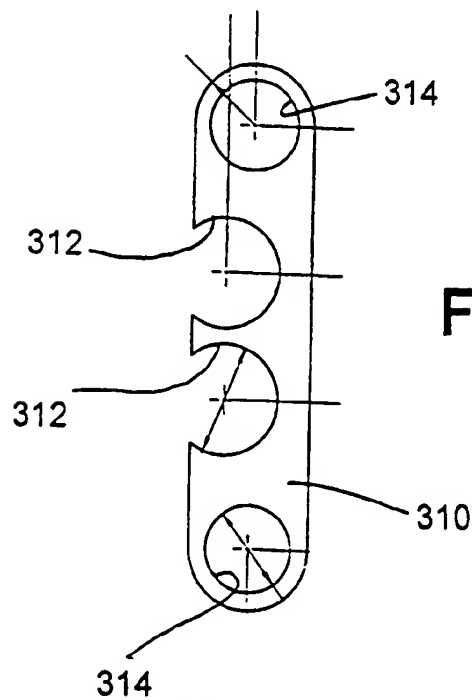
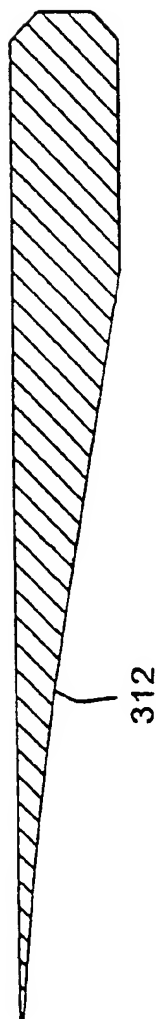


FIG. 38.

13/13

FIG. 41.



308

FIG. 40.

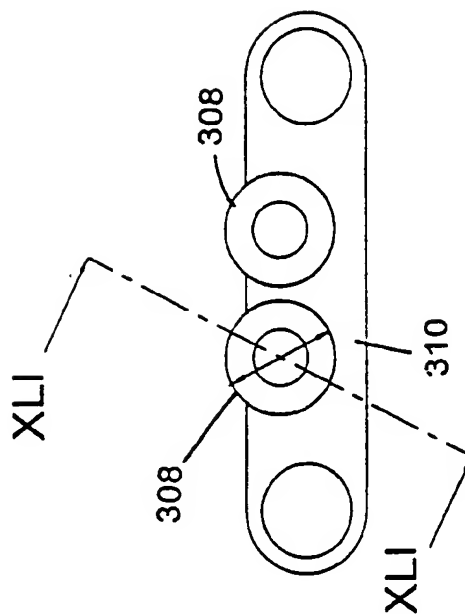
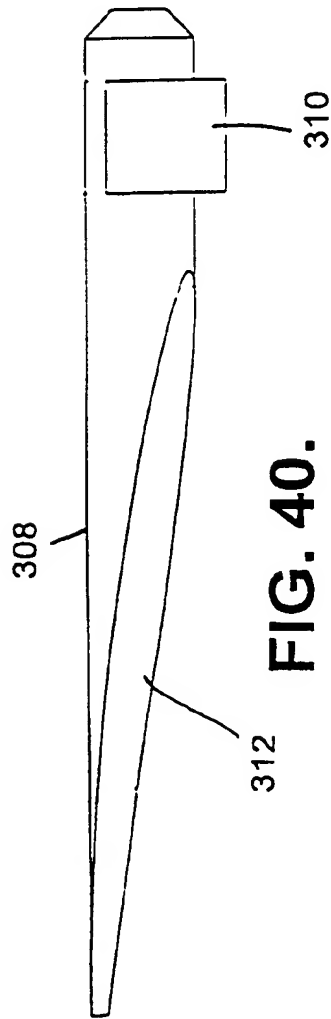


FIG. 39.

INTERNATIONAL SEARCH REPORT

International Application No

PCT/GB 98/03917

A. CLASSIFICATION OF SUBJECT MATTER

IPC 6 A61F2/16

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC 6 A61F

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 4 976 716 A (CUMMING J STUART) 11 December 1990 see column 3, line 43 - column 4, line 14; figures see column 7, line 11 - line 51	1
A	---	2-4
X	WO 95 24863 A (CUMMING J STUART) 21 September 1995 see abstract; claim 29; figures	1
A	---	2-4
A	WO 97 15253 A (STAAR SURGICAL CO INC) 1 May 1997 see page 12, line 1 - line 10; figures 29-31 see page 26, line 6 - line 10 ---	1-5, 13
	-/--	

☒ Further documents are listed in the continuation of box C.

☒ Patent family members are listed in annex.

* Special categories of cited documents :

"A" document defining the general state of the art which is not considered to be of particular relevance

"E" earlier document but published on or after the international filing date

"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)

"O" document referring to an oral disclosure, use, exhibition or other means

"P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.

"&" document member of the same patent family

Date of the actual completion of the international search

12 April 1999

Date of mailing of the international search report

19/04/1999

Name and mailing address of the ISA

European Patent Office, P.B. 5818 Patentlaan 2
NL - 2280 HV Rijswijk
Tel. (+31-70) 340-2040, Tx. 31 651 epo nl,
Fax: (+31-70) 340-3016

Authorized officer

Neumann, E

INTERNATIONAL SEARCH REPORT

International Application No

PCT/GB 98/03917

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 5 620 450 A (EAGLES DANIEL C ET AL) 15 April 1997 see the whole document -----	1,5,6,13

INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

PCT/GB 98/03917

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 4976716 A	11-12-1990	WO 9208423 A	29-05-1992
		US 5066297 A	19-11-1991
WO 9524863 A	21-09-1995	US 5578042 A	26-11-1996
WO 9715253 A	01-05-1997	US 5616148 A	01-04-1997
		US 5772666 A	30-06-1998
		AU 7476996 A	15-05-1997
		CA 2234002 A	01-05-1997
		CN 1200659 A	02-12-1998
		EP 0858304 A	19-08-1998
		US 5860984 A	19-01-1999
US 5620450 A	15-04-1997	US 5499987 A	19-03-1996
		US 5860984 A	19-01-1999
		AU 4749496 A	24-07-1996
		CA 2208997 A	11-07-1996
		CN 1172421 A	04-02-1998
		EP 0804131 A	05-11-1997
		JP 10511876 T	17-11-1998
		WO 9620662 A	11-07-1996
		US 5616148 A	01-04-1997
		US 5772666 A	30-06-1998
		AU 4501796 A	17-06-1996
		CA 2181472 A	30-05-1996
		CN 1143313 A	19-02-1997
		EP 0743840 A	27-11-1996
		JP 9508053 T	19-08-1997
		NZ 300317 A	26-06-1998
		WO 9615743 A	30-05-1996
		US 5807400 A	15-09-1998
		US 5728102 A	17-03-1998
		AU 1846395 A	04-09-1995
		CA 2183462 A	24-08-1995
		CN 1145580 A	19-03-1997
		EP 0901343 A	17-03-1999
		JP 9509086 T	16-09-1997
		NZ 281501 A	24-09-1998
		WO 9522287 A	24-08-1995
		EP 0746237 A	11-12-1996
		NZ 282170 A	26-06-1998
		AU 692425 B	11-06-1998
		AU 5349594 A	26-04-1994
		AU 6197498 A	13-08-1998
		CA 2144741 C	08-04-1997
		EP 0723429 A	31-07-1996
		JP 8505540 T	18-06-1996
		WO 9407436 A	14-04-1996
		US 5494484 A	27-02-1996
		US 5582614 A	10-12-1996
		US 5876440 A	02-03-1999
		US 5868751 A	09-02-1999
		US 5800442 A	01-09-1998